

MICROLEAKAGE EVALUATION OF MODIFIED MINERAL TRIOXIDE AGGREGATE EFFECT TOWARD MARGINAL ADAPTATION ON CERVICAL DENTIN PERFORATION

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ABSTRACT

Objective: To analyze the marginal adaptation of conventional MTA (ProRoot®MTA) and modified MTA (MTA Flow™) on perforated dentin.

Methods: Forty specimens of human's premolar teeth with lateral perforations were sealed by conventional MTA (n=20) and modified MTA (n=20). After 24 hours, the specimens were immersed in Indian ink for 24 hours, then embedded in resin and sectioned longitudinally in mesial-distal direction. The score of microleakage was determined using stereo microscope (SteREO Discovery. V12, Carl Zeiss) with 20x magnification. Statistical analysis was done by Chi Square (p<0,05).

Results: Less microleakage score (0,5-1mm) was detected in modified MTA (25%) compared to conventional MTA (45%), although not statistically significant.

Conclusion: Microleakage were detected in both conventional and modified MTA as material for cervical dentin perforation treatment, although modified-MTA group showed less microleakage score.

Keywords: Perforation, Mineral trioxide aggregate, Modified mineral trioxide aggregate, Microleakage, Marginal adaptation.

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INTRODUCTION

Perforation is a procedural accident that can occur during endodontic treatment to create communications between the root canal system and supporting tissues of the teeth. Sealing the perforation defect is an important step in limiting bacterial contamination [1]. Among the various available materials to seal perforations, MTA is the optimal choice for the procedure due to its biocompatibility, great sealing ability and adaptation to the dentinal wall, high pH, and ability to release calcium ions [2-4]. MTA applications can also induce hard tissue formation (dentin, cementum, and bone) and can facilitate periodontal tissue regeneration [2-5]. Pace *et al.* reported that 90% of perforation treatments using MTAs show periodontal and bone healing after 6 months, visible through the decrease in radiolucency in X-ray photos [5]. The material is not without disadvantages; however, namely, discoloration, lengthy setting times, and difficulty in handling [2,4].

Over time, modifications have been made to improve MTAs' undesirable properties. MTA discoloration was resolved with the release of white MTA (WMTA) in 2002, which contained less iron than the first version, gray MTA (GMTA), marketed originally in 1998 [3]. However, most marketed MTA products still have long setting times of typically 3-4 h [1,2,4]. New MTA-based materials, marketed under the name MTA Flow™ (Ultradent, South Jordan, UT), have also been developed to have smaller particle sizes. These are made up of powder and gel components with a particle size of powder at <10 µm. The mean particle size of the conventional ProRoot® MTA (Dentsply, Tulsa) is 10 µm, in which all particles are smaller than 50 µm [6]. Komabayasi *et al.* (2008) observed that the particle sizes of ProRoot® MTA (Dentsply, Tulsa) and MTA Angelus® (Angelus, Brazil) ranged between 1.5 and 160 µm, with the percentage of particles between 6 and 10 µm at 73% for ProRoot® MTA (Dentsply, Tulsa) and 53% for MTA Angelus® (Angelus, Brazil) [7].

MTA Flow™ (Ultradent, South Jordan, UT)'s basic materials and properties resemble those of conventional MTAs (e.g., they have the same indications because they share the same active ingredient) [8].

The possible advantages of MTA Flow™ (Ultradent, South Jordan, UT) over a conventional MTA have yet to be researched in depth, however. Thus, it is necessary to conduct further analysis of MTA modifications, particularly in regards to the material's marginal adaptation. The aim of this study, therefore, is to analyze the differences in marginal adaptation between conventional and modified MTAs through microleakage evaluation in perforation treatments.

METHODS

Forty specimens of extracted human premolar teeth with no caries, fillings, crowns, root defects, or history of endodontic treatment were used for the present study. All teeth were kept moist before and during the experiment. The specimens were prepared through access opening and lateral perforation simulation. Perforations 2 mm in diameter were created by inserting a diamond round bur at 1 mm under the cemento-enamel junction (CEJ) to penetrate the proximal wall. The specimens were then divided randomly into two groups of 20 specimens. Those in the first group were sealed by a conventional MTA (ProRoot® MTA, Dentsply), and those in the second group were sealed by a modified MTA (MTA Flow™, Ultradent, South Jordan, UT). MTA manipulations were performed according to the manufacturer's instructions (powder: liquid ratio 3:1 for the first group and 2:2 for the second group); then, access cavity was sealed by glass ionomer cement (GIC) (GIC Fuji IX™, GC Corp Inc, USA). A dental loupe with ×3.0 magnification was used by the operator in all the procedures.

After 24 h in a 37°C incubator, the specimens were coated with nail polish, leaving 1 mm around the restoration at the proximal wall. The specimens were immersed in India ink for 24 h, then embedded in resin and sectioned longitudinally in a mesial-distal direction (Struers-Accutom-2). Microleakage scores were determined by measuring the depth of the ink's penetration along the restorations using a stereomicroscope (SteREO Discovery, V12, Carl Zeiss) with ×20 magnification. Statistical analyses were performed through Chi-square tests (p<0.05) using SPSS 20.0 software. A scanning electron microscope

(SEM) and energy dispersive spectroscopy (EDS) were applied to each group to observe their marginal adaptation (physical properties) and mineral release (chemical properties).

RESULTS

Microleakage data were obtained by measuring India ink penetration with a stereomicroscope ($\times 20$ magnification). Microleakage scores were determined as 0 = no leakage; 1 = leakage ranging between 0 and 0.5 mm; 2 = leakage ranging between 0.5 and 1 mm; and 3 = leakage more than 1 mm. The microscopic imaging of India ink penetration in Group 1 (conventional MTA) and Group 2 (modified MTA) was shown in Figs. 1 and 2.

Table 1 summarizes that 30% of Group 1 and 40% of Group 2 had no leakage (score 0), 25% of Group 1 and 35% of Group 2 had scores of 1, 45% of Group 1 and 25% of Group

2 had scores of 2, and neither group contained scores of 3. The Chi-square statistical analysis revealed no statistically substantial differences in microleakage scores between the conventional and modified MTAs ($p=0.414$), as shown in Table 1. SEM imaging ($\times 200$ magnification) revealed a gap between dentin and materials in both the conventional and modified MTAs (see Figs. 3 and 4). The EDS results confirmed that calcium ion release was higher in the modified MTA group (mean: 10.26%) than in the conventional MTA group (mean: 8.9%).

DISCUSSION

The India ink penetration revealed gaps or spaces between the dentinal wall of the root canal and sealant material in both the samples with conventional MTA and modified MTA. Leakages of varying degrees (i.e. different scores) were observed on the outlines of the longitudinal cuts on some samples, as shown in Table 1. Examination of the results shown in Table 1 showed that the largest number of those using the conventional MTA as their sealant for perforation scored a 2 (45%), with leakage ranging between 0.5 and 1 mm.

In the modified MTA group, the samples with scores of 0 (meaning no leakage) formed the largest result group (40%), followed by those with scores of 1 with leakage ranging between 0 and 0.5 mm (35%). These results indicate that less microleakage occurred in the modified MTA group than in the conventional MTA group.

This result is largely due to the particle size of the modified MTA, which was homogenous and smaller than 10 μm .

This falls in line with research conducted by Reyes-Carmona *et al.*, who concluded that material with more homogenously sized particles will yield higher mechanical binding [9].

The authors asserted that smaller particle sizes also minimize spacing between particles, increase surface area, and better interlock powder particles to improve integrity, making the material more resistant to liquid penetration (Fig. 5) [2,10].

These smaller particle sizes also take on a pasta-like consistency that is much easier to apply than conventional MTAs that are characterized by a granular, sand-like texture [7,9]. The statistical Chi-square testing revealed no substantial differences in microleakage between the conventional and modified MTAs used as sealants for perforation. This result is similar to that in research by Dimitrova *et al.*, on eight silicate calcium-based materials (MTA Angelus® [Angelus, Brazil], ProRoot MTA® [Dentsply, Tulsa], Aureoseal® [OGNA, Italy], Bio-Aggregate® [Diadent, Canada], Biodentin® [Septodont, USA], and Portland cements), which exhibited 5.62–7.28 μm leakage gaps between the material and dentin.

In this research, the smallest gap was observed on Bio-Aggregate® (Diadent, Canada) material and the biggest gap on other Biodentin® (Septodont, USA) but overall there were no statistical differences

Table 1: Microleakage score distribution in conventional and modified MTA groups

Materials	Microleakage scores (%)				p
	0	1	2	3	
Conventional MTA (n=20)	6 (30)	5 (25)	9 (45)	0 (0)	0.414
Modified MTA (n=20)	8 (40)	7 (35)	5 (25)	0 (0)	

MTA: Mineral trioxide aggregate

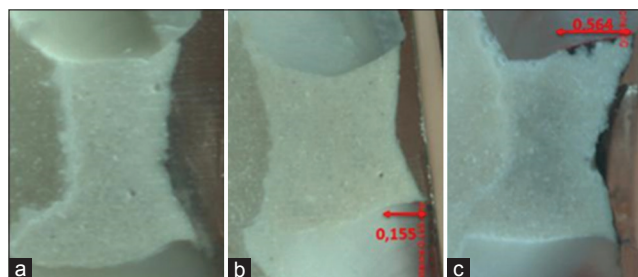


Fig. 1: Stereomicroscope pictures of conventional mineral trioxide aggregate group (a) score 0, (b) score 1, and (c) score 2

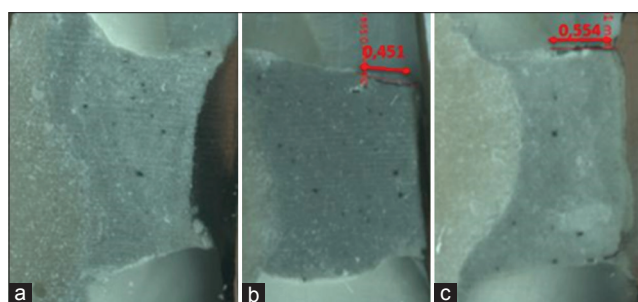


Fig. 2: Stereomicroscope pictures of modified mineral trioxide aggregate group (a) score 0, (b) score 1, and (c) score 2

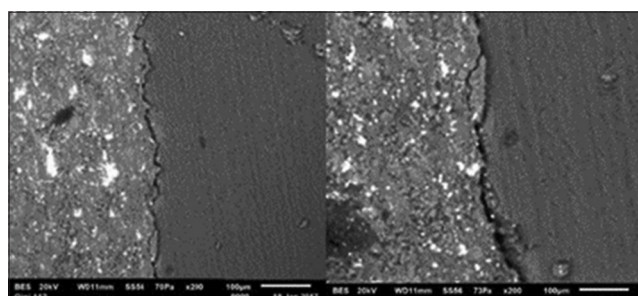


Fig. 3: Scanning electron microscope pictures ($\times 200$) of longitudinally sectioned specimens with a gap between the dentin and conventional mineral trioxide aggregate

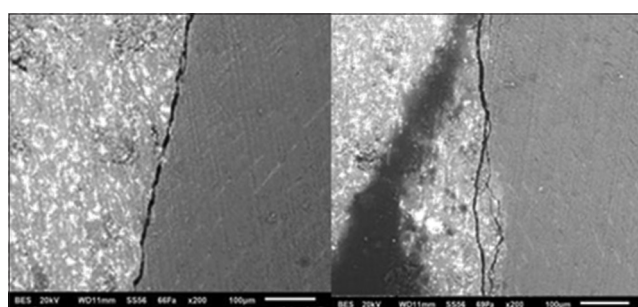


Fig. 4: Scanning electron microscope pictures ($\times 200$) of longitudinally sectioned specimens with a gap between the dentin and modified mineral trioxide aggregate

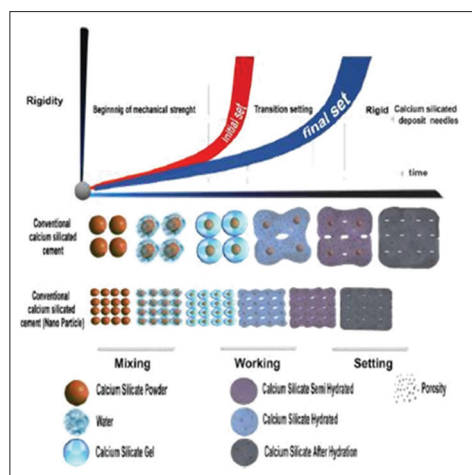


Fig. 5: Schematic figure of the mixing, working, and setting phases of calcium silicate cement. Materials with smaller size particles show less porosity than materials with large particles [10,16].

among the samples [11]. The present research used the conventional ProRoot® MTA (Dentsply, Tulsa) on the first group, as this material is the current standard for treating perforation, and the modified MTA Flow™ (Ultradent, South Jordan, UT), with its more homogeneously sized particles at <math><10\ \mu\text{m}</math>, on the second group.

In the present study, the modified MTA was observed to have a better consistency, making it easier to apply as well as a faster setting time of 15 min. Indeed, after a mere 5 min, the cement layer was able to be rinsed and dried without dissolving [8]. This faster setting time was due to the modified MTA's smaller particle size than that of the conventional MTA. This is in line with a study conducted by Saghiri *et al.*, who shrunk a WMTA to make it more reactive. The smaller size meant more contacted surface, thus speeding up the setting time from 43 ± 2 min to 6 ± 1 min. This eliminated the need to wash the outer layer of the MTA [2]. According to the literature, MTAs are desirable as perforation sealants because of the difficulty in isolating the working condition and the risk of blood and gingival fluid overflowing after application.

The dye penetration method was used to make microleakages observable in the present study. Sample teeth were immersed in coloring dye for a certain amount of time, then cut and observed at the marginal level between tooth and material. The dye used for this method was India ink with a particle diameter of $\leq 3\ \mu\text{m}$, smaller than the diameter of the bacteria found inside the canal spaces of the sample teeth [12]. Coloration on the marginal level of a sample tooth meant the presence of a microleakage. Verissimo and Fabinelli described dye penetration as the most common method for such procedures because of its easy application and lack of chemical reactions [12].

Under moist conditions, an MTA will initiate physical binding with dentin by forming a micromechanical tag-like structure in the dentinal tubules as well as chemical binding by forming an amorphous structure of silicate calcium with the dentinal wall. It also induces the formation of solid tissue surrounding the MTA [2]. This mirror study conducted by Dreger *et al.* in which MTA and Portland cement leached into the tissue calcium and phosphate ions capable of stimulating mineral deposition in the cement-dentin interface and in the interior of the dentinal tubules [13]. Continuous precipitation of calcium and phosphate ions causes hydroxyapatite to form on the interfacial layer and eventually bond biologically with the dentinal wall, which also has hydroxyapatite as its main structure [14]. Bird *et al.*, who evaluated the ability of MTAs to penetrate human dentinal tubules, concluded that physiochemical reactions initiate the gradual formation of hydroxyapatite between an MTA and dentin, improving the MTA's sealing ability and biocompatibility [6]. These results all demonstrate that MTAs with

smaller particle sizes and a more fluid consistency can better fill the irregularities of a dentinal wall to minimize gaps and that this can be done even faster with hydroxyapatite formation. Further, a WMTA modified by Saghiri *et al.* had nanoscale-sized particles that increased the calcium ion release significantly, affecting hard tissue regeneration to a high degree [10]. Calcium ions also influence tissue mineralization by fastening cell proliferation when present in large quantities [15]. The modified MTA in the present study demonstrated improved hard tissue regeneration potential (as shown in the results of the EDS tests), confirming that calcium ion release is higher in modified MTAs.

The SEM images presented in Figs. 3 and 4 show the gaps in both material groups. The calcium and phosphate ion precipitation had not yet maximized for sealing, as the observation took place 24 h after the MTA was applied. Kouzmanova made the same observation of such gaps 24 h after applying a silicate calcium-based material, including an MTA, to a bifurcation perforation [11]. Another study by Sarkar showed that bonding between an MTA and dentin will form a perfect seal over such gaps as an interfacial layer consisting of a new hydroxyapatite composition once 2 months has elapsed since MTA application to the canal space [14]. In short, the findings in the literature and in the present study indicate that modification increases not only the physical but also the chemical properties of an MTA. This process is driven by increases in marginal adaptation and ion calcium release as observed found in the present study.

CONCLUSIONS

Microleakages were detected in both conventional and modified MTAs used as materials for treating cervical dentin perforations, though the modified MTA group exhibited slightly lower microleakage scores.

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